

A brain-computer interface for mental arithmetic task from single-trial near-infrared spectroscopy brain signals

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Abstract

Near-infrared spectroscopy (NIRS) enables non-invasive recording of cortical hemoglobin oxygenation in human subjects through the intact skull using light in the near-infrared range to determine. Recently, NIRS-based brain-computer interfaces are introduced for discriminating left and right-hand motor imagery. A neuroimaging study has also revealed event-related hemodynamic responses associated with the performance of mental arithmetic tasks. This paper proposes a novel BCI for detecting changes resulting from increases in the magnitude of operands used in a mental arithmetic task, using data from single-trial NIRS brain signals. We measured hemoglobin responses from 20 healthy subjects as they solved mental arithmetic problems with three difficulty levels. Accuracy in recognizing one difficulty level from another is then presented using 5×5-fold cross-validations on the data collected. The results yielded an overall average accuracy of 71.2%, thus demonstrating potential in the proposed NIRS-based BCI in recognizing difficulty of problems encountered by mental arithmetic problem solvers.

1. Introduction

Brain-Computer Interface (BCI) is a communication system that directly translates brain signals into commands for controlling an external device [1]. Methods for measuring brain signals include electroencephalography (EEG), functional magnetic resonance imaging (fMRI), magnetoencephalography (MEG), positron emission tomography (PET), and

more invasive methods such as electrocorticogram (ECoG) and implanted electrodes [1]. Recently, the feasibility of using near infrared spectroscopy (NIRS) in the development of BCIs for left and right-hand motor imagery has been demonstrated [2], [3]. Although various methods exist, only EEG and NIRS are suitable for widespread everyday use since MEG, fMRI and PET are technically complex, expensive and have limited real-time capabilities [4].

NIRS is a non-invasive optical neural imaging technique that measures concentration changes of oxyhemoglobin (HbO₂) and deoxyhemoglobin (Hb) in the cerebral vessels by means of different absorption spectra in the near infrared range [5]. The suitability of recognizing left and right motor imagery from hemodynamic responses for developing BCI was first demonstrated in [6], and later in [2], [3]. However, studies have shown that other cognitive tasks, such as mental arithmetic, generally cause an increase of HbO₂ associated with decreases of Hb in the prefrontal cortex [7]. There are recent seminar papers that investigated hemodynamic response using NIRS on mental arithmetic tasks [8], [9], and the recognition of mental workload from NIRS signals [10], [11]. To the best of the authors' knowledge, there is currently no NIRS-based BCI designed to recognize the problem size in mental arithmetic tasks. The motivation behind the investigation is that the amplitude of an event-related brain potentials has been shown to be modulated by the size of operands in mental arithmetic tasks [12].

This paper proposes a novel BCI for recognizing the size of operands in a mental arithmetic task from single-trial NIRS brain signals, and presents preliminary results from a study on 20 healthy subjects.

2. Methodology

This section describes how the NIRS brain signal is collected, how the hemodynamic responses are computed, and the methodology for recognizing the operand size from the hemodynamic responses in the proposed NIRS-based BCI.

2.1. Data collection protocol

The data was collected from 20 healthy, right-handed participants (12 male, 8 female; mean age=24.7 years, range 19–30). All subjects had no neurological injury, completed at least 12 years of education, were fully informed, and consented to participate in the study. The subjects were seated in a comfortable chair in a room with normal lighting and were asked to relax before the experiment commenced. They were also asked to minimize movement and to respond as quickly and correctly as possible during data collection. The recording session for each subject was less than 30 mins.

During data collection, the subjects underwent a total of 75 trials of arithmetical tasks that were evenly distributed into 3 difficulty levels: easy, medium, and hard. The subjects performed two single-digit additions (e.g. 5 + 4) for the easy tasks, single-digit and double-digits additions (e.g. 5 + 34) for the medium tasks, and two double-digits additions (e.g. 53 + 34) for the hard tasks. Arithmetical tasks that involved the carry-over operation are one of the contributing factors of problem size effect. Hence these tasks were excluded. 5 trials of the same difficulty level formed a block and a total of 15 randomized blocks were presented to the subjects. The duration of each trial was 12 s. At the start of each trial, the arithmetic task was presented at the center of a display screen and remained for a maximum of 9 s or until the subject responded. After the subject responded, a fixation cross appeared for the remainder of the 12 s duration. After completing 1 block, a fixation cross would appear for 30 s before the next block began.

The data were collected using 16-channel continuous-wave near infrared spectroscopy (see Fig. 1) device to compute hemodynamic changes in the prefrontal cortex while performing the mental arithmetic tasks. The probes comprised 4 tri-wavelength (730nm 805nm, and 850nm) LEDs and 10 detectors held onto the subject's forehead using a Velcro band. The 730nm wavelength was used to detect deoxy Hb, 850nm to detect oxy Hb, and 805nm to detect the dark current or fixed-pattern noise. A total of 16 channels was collected for each wavelength using a sampling frequency of 3 Hz. This yielded a total of

32 channels of concentration changes in deoxyhemoglobin (HB) and oxyhemoglobin (HBO₂).

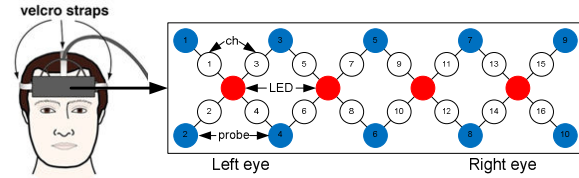


Fig. 1 Multichannel near infrared optodes arrangement on the prefrontal cortex for the study. A pair of LED and probe yields 1 channel of HB and 1 channel of HBO₂ signal. A total of 16 channels of HB and 16 channels of HBO₂ signals are thus collected.

2.2. Preprocessing

Let the optical density for wavelength λ acquired from a set of source and detector labeled as channel c be denoted as OD_c^λ . First, the optical densities for wavelength $\lambda_1=730\text{nm}$ and $\lambda_2=850\text{nm}$ are subtracted from wavelength 805nm to remove the fixed-pattern noise. Next, the relative change in optical density is computed by dividing each time sample by the mean of the optical signal acquired for the session [2] given by

$$\overline{\Delta OD}_c^\lambda(t) = OD_c^\lambda(t) / \frac{1}{T} \sum_{\tau=1}^T OD_c^\lambda(\tau), \quad (1)$$

where $\overline{\Delta OD}_c^\lambda$ is the normalized change in optical density, and T is the total number of time samples acquired for the session.

$\overline{\Delta OD}_c^\lambda$ is then low-pass filtered using Chebychev type II filter with a cut-off frequency of 0.14 Hz and pass-band attenuation of 0.02 dB. Next, linear-detrending is performed to remove the drift (low frequency bias) in the NIRS measurements due to various reasons, such as subject movement, blood pressure variation, and instrumental instability [13]. After filtering and detrending, unity is added to bring the mean of the optical density to unity instead of zero. The change in optical density ΔOD_c^λ is then computed as the negative logarithm from the resultant given by

$$\Delta OD_c^\lambda = -\log\left(\widetilde{\Delta OD}_c^\lambda\right), \quad (2)$$

where $\widetilde{\Delta OD}_c^\lambda$ denotes the filtered, linearly-detrended optical density with unity added.

2.3. Computing hemodynamic responses

In NIRS studies, optical density changes ΔOD_c can be expressed as a linear combination of the changes in oxyhemoglobin $\Delta[\text{HbO}_2]_c$ and deoxyhemoglobin $\Delta[\text{Hb}]_c$. This equation, referred to as the modified Beer-Lambert law (MBLL) [5], [14], is given by

$$\Delta OD_c^\lambda = L^\lambda \text{DPF}^\lambda \left(\varepsilon_{\text{Hb}}^\lambda \Delta[\text{Hb}]_c + \varepsilon_{\text{HbO}_2}^\lambda \Delta[\text{HbO}_2]_c \right), \quad (3)$$

where ε^λ is the wavelength-dependent extinction coefficient, L^λ is the path length from source to detector, and DPF^λ is the differential path-length.

Typically, dual wavelength measurements of optical absorption are often converted to changes in HbO_2 and Hb by solving the series of linear equations [2]

$$\begin{bmatrix} \Delta[\text{HbO}_2]_c \\ \Delta[\text{Hb}]_c \end{bmatrix} = (\mathbf{E}^T \mathbf{E})^{-1} \mathbf{E}^T \begin{bmatrix} \Delta\text{OD}_c^{\lambda_1} / L^{\lambda_1} \text{DPF}^{\lambda_1} \\ \Delta\text{OD}_c^{\lambda_2} / L^{\lambda_2} \text{DPF}^{\lambda_2} \end{bmatrix}, \quad (4)$$

where

$$\mathbf{E} = \begin{bmatrix} \varepsilon_{\text{HbO}_2}^{\lambda_1} & \varepsilon_{\text{Hb}}^{\lambda_1} \\ \varepsilon_{\text{HbO}_2}^{\lambda_2} & \varepsilon_{\text{Hb}}^{\lambda_2} \end{bmatrix}. \quad (5)$$

2.4. Feature extraction

Feature extraction is performed by taking the average $\Delta[\text{HB}]_c$ and $\Delta[\text{HBO}_2]_c$ across 12s of NIRS data recorded for a single trial. Since there are 16 channels, this resulted in a total of 32 features for a single trial.

The above feature extraction is compared with the method in [11] that employed features using averaged ΔHB and ΔHBO_2 from the left and right side of the prefrontal cortex. This method is implemented by averaging ΔHB and ΔHBO_2 from channels $c = 1, 2, 3$ and 4 for the left and channels $c = 13, 14, 15$ and 16 for the right in this work. This resulted in four time series features $\Delta[\text{HB}]_{\text{left}}$, $\Delta[\text{HBO}_2]_{\text{left}}$, $\Delta[\text{HB}]_{\text{right}}$ $\Delta[\text{HBO}_2]_{\text{right}}$ for each trial. Taking the average across 12s of NIRS data resulted in a total of 4 features for a single trial.

The feature vector for a trial i^{th} trial is formed using

$$\mathbf{x}_i = [\Delta[\text{HbO}_2] \quad \Delta[\text{Hb}]], \quad (6)$$

where $\mathbf{x}_i \in \mathbb{R}^{1 \times \text{nt}}$, $i=1,2,\dots,\text{nt}$; nt denotes the total number of trials in the training data.

The feature matrix from training data is then

$$\mathbf{X} = [\mathbf{x}_1 \quad \mathbf{x}_2 \quad \dots \quad \mathbf{x}_{\text{nt}}]^T. \quad (7)$$

2.5. Feature selection and classification

Feature selection is then performed to select discriminative features using the Mutual Information-based Best Individual Feature (MIBIF) algorithm [15] on the training data. The MIBIF algorithm first computes the mutual information of each feature with the class labels. The mutual information between the features $\mathcal{F} = \{f_1, f_2, \dots, f_{\text{nt}}\}$ whereby f_j comprises the j^{th} column of \mathbf{X} , and the class \mathcal{C} can be represented as [16]

$$I(\mathcal{F}; \mathcal{C}) = H(\mathcal{C}) - H(\mathcal{C} | \mathcal{F}) \quad (8)$$

The mutual information of each feature $I(f_j, \mathcal{C})$ can be computed by estimating the entropy and the

conditional entropy using Parzen Window [16], [17]. The features are then sorted in descending mutual information and the first k features are then selected.

Next, the Naïve Bayesian Parzen Window (NBPW) classifier [15] is used to classify the selected features. The NBPW classifier estimates conditional probability $p(\mathbf{x}|\omega)$ using Parzen Window and prior probability $P(\omega)$ from training data samples, then predicts the class ω with the highest posterior probability $p(\omega|\mathbf{x})$ given a test sample \mathbf{x} using Bayes rule and the naïve assumption that all the features are conditionally independent.

3. Experimental Results

The performance of the proposed NIRS-based BCI using the feature extraction techniques described in section 2.4 are evaluated using 5x5-fold cross-validations on the single-trial NIRS data collected. Feature selection and training of the classifier are performed on the training data, and classification performance is then evaluated on the test data in each fold. The performance is evaluated on two of three difficulty levels and the results are presented in TABLE I. The averaged performance of each feature extraction technique is presented in the last row.

TABLE I

Results for Easy versus Hard (*EvH*), Easy versus Medium (*EvM*), Medium versus Hard (*MvH*); using Averaged Left and Right HB, HBO2 channels (*AvgLRch*), using MIBIF to select 2 of *AvgLRch* (*Best2AvgLRch*), using MIBIF to select 4 out of 32 channels of HB, HBO2 (*Best4ch*); and using MIBIF to select 5 channels (*Best5ch*)

	<i>AvgLRch</i>		<i>Best2AvgLRch</i>		<i>Best4ch</i>		<i>Best5ch</i>					
Sub	<i>EvH</i>	<i>EvM</i>	<i>MvH</i>	<i>EvH</i>	<i>EvM</i>	<i>MvH</i>	<i>EvH</i>	<i>EvM</i>	<i>MvH</i>			
1	74.0	70.0	72.8	67.6	56.8	70.0	70.0	69.6	73.6	72.0	68.8	75.6
2	76.0	86.0	68.0	77.2	86.0	65.2	76.8	84.8	79.6	76.4	86.8	80.0
3	52.8	63.2	70.4	51.6	64.4	66.0	67.6	66.4	70.4	70.8	69.2	72.8
4	73.2	74.4	63.2	70.4	69.2	52.0	68.0	76.8	67.6	68.8	74.8	70.8
5	72.8	73.2	70.4	67.2	74.8	59.2	68.8	76.4	72.0	67.2	74.8	73.2
6	65.2	74.0	67.6	64.4	75.6	59.6	69.2	73.6	70.8	69.2	73.2	71.2
7	56.8	57.6	50.4	48.4	53.2	48.0	53.6	64.0	55.6	54.0	63.2	60.0
8	62.4	70.4	66.8	60.8	61.6	67.6	67.6	64.4	63.2	64.8	71.2	64.4
9	72.4	70.4	65.2	70.0	66.4	61.6	81.6	78.4	78.4	79.6	79.2	76.4
10	72.4	59.6	63.2	73.2	60.4	55.6	70.4	72.0	73.2	71.6	72.8	72.4
11	60.0	56.0	69.6	53.6	54.0	64.8	61.6	68.0	78.8	62.8	71.2	78.4
12	66.4	64.8	71.6	70.0	63.2	69.6	66.0	62.0	70.4	67.2	64.4	70.8
13	50.4	54.4	56.4	54.4	50.0	46.0	66.0	60.8	61.2	66.8	64.8	62.8
14	60.4	53.6	53.6	53.6	50.4	52.0	62.8	68.0	67.2	61.2	70.4	66.8
15	52.0	63.2	61.6	50.4	66.8	65.2	71.6	65.2	67.6	70.8	62.8	68.4
16	65.2	57.2	72.0	68.8	53.2	72.4	69.6	72.4	72.0	71.2	72.4	74.8
17	65.6	62.4	60.0	64.8	62.0	58.0	65.6	77.6	56.4	66.8	74.4	55.2
18	65.6	74.8	62.0	56.8	79.6	63.6	74.8	82.4	70.4	81.2	82.4	68.4
19	49.2	60.0	53.6	44.0	60.4	45.6	64.8	68.4	68.4	60.0	70.0	70.0
20	70.8	71.2	62.8	73.2	75.2	60.8	91.6	92.4	84.0	92.8	91.6	84.4
Avg	64.2	65.8	64.1	62.0	64.2	60.1	69.4	72.2	70.0	69.8	72.9	70.8
	64.7			62.1			70.5			71.2		

Statistical analysis using 1-way ANOVA on the

results of the proposed NIRS-based BCI using different feature extraction techniques in TABLE I revealed significant differences ($p=1.87\times 10^{-10}$). Selecting 2 features extracted by averaging ΔHB and ΔHBO_2 from left and right channels using the MIBIF algorithm yielded significantly poorer results from t -test compared to all features ($\mu=64.7\%$ from *AvgLRch* versus 62.1% from *Best2AvgLRch*, $p=1.84\times 10^{-5}$). In contrast, selecting 4 features extracted by averaging ΔHB and ΔHBO_2 across each individual channels yielded significantly better results than averaging ΔHB and ΔHBO_2 from left and right channels (mean 70.5% from *Best4ch*, $p=2.66\times 10^{-9}$). Increasing the features selected to 5 significantly improved the results further ($\mu=71.2\%$ from *Best5ch*, $p=0.03$), but further increase to 6 did not yield significantly improved results ($\mu=71.55\%$, $p=0.16$, *Best6ch* omitted from TABLE I).

4. Conclusions

This paper presents a novel BCI for detecting the problem size effect in a mental arithmetic task from single-trial NIRS brain signals. A study is performed on 20 healthy subjects to measure changes in the concentration of oxyhemoglobin (ΔHBO_2) and deoxyhemoglobin (ΔHB) responses in performing three difficulty levels of mental arithmetic. The performance of the proposed NIRS-based BCI is evaluated using 5×5 -fold cross-validations on the single-trial NIRS data collected using various features extraction methods. The results showed that performing feature selections on ΔHB and ΔHBO_2 from all the channels yielded an averaged accuracy of 71.2% , which is significantly better than using features by averaging ΔHB and ΔHBO_2 from the left and right side of the prefrontal cortex. The results demonstrated the potential of the proposed NIRS-based BCI for recognizing the problem size effect in mental arithmetic task. More advanced feature selection and classification methods could be employed to further improve the classification performance.

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